



**COMMITTEE ON MEDICINAL PRODUCTS FOR HUMAN USE
(CHMP)**

DRAFT

**GUIDELINE ON THE REQUIREMENTS FOR CLINICAL DOCUMENTATION FOR
ORALLY INHALED PRODUCTS (OIP) INCLUDING THE REQUIREMENTS FOR
DEMONSTRATION OF THERAPEUTIC EQUIVALENCE BETWEEN TWO INHALED
PRODUCTS FOR USE IN THE TREATMENT OF ASTHMA AND CHRONIC
OBSTRUCTIVE PULMONARY DISEASE (COPD)**

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GUIDELINE ON THE REQUIREMENTS FOR CLINICAL DOCUMENTATION FOR ORALLY INHALED PRODUCTS (OIP) INCLUDING THE REQUIREMENTS FOR DEMONSTRATION OF THERAPEUTIC EQUIVALENCE BETWEEN TWO INHALED PRODUCTS FOR USE IN THE TREATMENT OF ASTHMA AND CHRONIC OBSTRUCTIVE PULMONARY DISEASE (COPD)

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1 EXECUTIVE SUMMARY

2 This guideline is a revision of the *CPMP Points to Consider on the Requirements for Clinical*
3 *documentation for Orally Inhaled Products (OIP) CPMP/EWP/4151/00*. It clarifies the requirements
4 for clinical documentation for abridged applications of orally inhaled formulations and
5 variations/extensions to a marketing authorisation in respect of the demonstration of therapeutic
6 equivalence between two inhaled products for use in the management and treatment of asthma and
7 chronic obstructive pulmonary disease.

8 1. INTRODUCTION (background)

9 This guideline describes the clinical requirements for inhalation products further to the
10 pharmaceutical considerations laid down in the *CHMP Guideline on the Pharmaceutical*
11 *Quality of Inhalation and Nasal Products EMEA/CHMP/QWP/49313/2005corr*.

12 2. SCOPE

13 Existing CHMP documents which discuss the clinical requirements for the development of inhaled
14 products - *Note for Guidance on the Clinical Investigation of Medicinal Products in the Treatment of*
15 *Asthma CPMP/EWP/2922/01* and *Points to Consider on Clinical Investigation of Medicinal Products*
16 *in the Chronic Treatment of Patients with Chronic Obstructive Pulmonary Disease (COPD)*
17 *CPMP/EWP/562/98* - discuss primarily the development of new active substances. This guideline is
18 directed particularly at the requirements for demonstration of therapeutic equivalence between two
19 inhaled products, in the context of either abridged applications or variations/extensions to a marketing
20 authorisation, used in the treatment and management of patients with asthma and/or COPD.

21 This guideline will address data required which are often dependent on the performance of the device
22 from which the active substance is inhaled. This document will address specific issues of relevance to
23 inhaler devices but may not be able to offer complete guidance on every aspect of the clinical
24 documentation for the product.

25 Further to clinical performance in respect of the clinical efficacy and safety of the product
26 administered via the inhaler device, knowledge of the *in vitro* performance, and particularly the flow-
27 dependent particle size distribution of the product, is important and will have some influence on the
28 clinical development programme.

29 This guideline is relevant for medicinal products administered via:

- 30 • pressurised metered dose inhalers
- 31 • pressurised metered dose inhalers with spacer devices and holding chambers
- 32 • breath-operated inhalers
- 33 • non-pressurised, pump activated, liquid reservoir metered dose inhalers
- 34 • dry powder inhalers using a reservoir and metering mechanism
- 35 • dry powder inhalers using a pre-dispensed dose
- 36 • solutions and suspensions for nebulisation

37 3. LEGAL BASIS

38 This guideline has to be read in conjunction with the introduction and general principles and part I, II
39 of the Annex I to Directive 2001/83/EC as amended and Commission Regulation (EC) No 1085/2003.
40 In particular, this guideline has to be seen as additional to the following existing CHMP Guidance:

- 41 - *EMEA/CHMP/QWP/49313/2005corr: Guideline on the Pharmaceutical Quality of Inhalation*
42 *and Nasal Products*
- 43 - *CPMP/EWP/239/95: Note for Guidance on the Clinical Requirements for Locally Applied,*
44 *Locally Acting Products Containing Known Constituents*
- 45 - *CPMP/180/95: Guideline for PMS Studies for Metered Dose Inhalers with New Propellants*
- 46 - *CPMP/EWP/240/95: Note for Guidance on Fixed Combination Medicinal Products*

- 47 - CPMP/III/5378/93-Final: Note for Guidance: Replacement of Chlorofluorocarbons (CFCs) in
48 Metered Dose Inhalation Products
- 49 - CPMP/ICH/363/96: Note for Guidance on Statistical Principles for Clinical Trials
- 50 - CPMP/EWP/QWP/1401/98 Note for guidance on the investigation of bioavailability and
51 bioequivalence

52 The existing CHMP Guidance referred to in the first paragraph in section 2 above and which discuss
53 primarily requirements for the development of new active substances, may also need to be considered.

54 **4. MAIN GUIDELINE TEXT**

55 **4.1 INHALATION DEVICES AND CLINICAL REQUIREMENTS**

56 Propellant-containing pressurised metered dose inhalers, dry powder inhalers and nebulisers have
57 different flow-dependent pulmonary deposition patterns. Handling of these devices – and the resultant
58 patient preference – differs. Therefore some general considerations concerning the requirements for
59 clinical documentation in respect of these devices are presented below.

60 **4.1.1 Pressurised metered dose inhalers**

61 Pressurised metered dose inhalers (pMDIs) contain different propellants and other excipients, and may
62 use different valve systems, all of which may result in differing clinical outcomes. The standard pMDI
63 requires co-ordination of actuation of the device with inspiration of breath; breath-operated devices
64 and spacing devices remove the need for such co-ordination. Spacing devices are considered necessary
65 for use with all pMDIs, and should always be used when a pMDI is used by a child. Appropriate data
66 to support the use of a specific named spacing device with a pMDI containing a specific active
67 substance or specific combination of active substances must be included in the dossier submitted in
68 support of all applications for marketing authorisations for such products (see also section 4.1.1.2).

69 When a new propellant or excipient is introduced into a pMDI the possible impact on clinical efficacy
70 and safety must be studied in addition to any toxicological and preclinical programme (see section
71 4.7). Generation of extended safety data may be necessary. In respect of safety, local tolerability must
72 be assessed and any evidence of increased bronchial hyperreactivity or paradoxical bronchospasm
73 must be sought. It may be necessary to also assess any effect that the new propellant or excipient may
74 have on mucociliary clearance.

75 **4.1.1.1 Breath-operated inhalers**

76 A minimal peak inspiratory flow rate (PIFR) is required to trigger a breath-operated inhaler (BOI) and
77 if this minimal PIFR cannot be achieved by the patient, inhaler use will be unsuccessful. Therefore,
78 the clinical programme has to include relevant data regarding the PIFR required to trigger the BOI and
79 discussion of those patient groups who would normally be able to produce a sufficient PIFR to trigger
80 the device and those patient groups who may have problems (for example patients with severe asthma,
81 patients suffering from an acute attack of asthma, small children, etc). The relevant patient population
82 must be adequately investigated and subsequently defined in order that the prescriber can be assured
83 that the product is only prescribed to and used by suitable patient groups.

84 The reference product for a BOI can be the corresponding pMDI. However it must be demonstrated
85 that the target populations can generate the same flow rates through the BOI and pMDI and therefore
86 that all patients can trigger both devices successfully (see section 4.2).

87 For inhalers that can be breath-operated and hand-operated patients need an explanation in the
88 package leaflet as to how to recognise an inadequate breath-operated inhalation and how and when to
89 switch to a hand-operated inhalation procedure. The two modes of action should be compared using
90 the parameters outlined below (see section 4.2) to determine whether there is a need for clinical data to
91 support each method of inhalation.

92 4.1.1.2 Spacing devices and holding chambers

93 Spacing devices are usually expected to facilitate inhalation via a pMDI and decrease the amount of
94 medicinal product deposited in the mouth and pharynx and subsequently swallowed. The use of a
95 spacing device is recommended for all patients in principle but particularly for those who find co-
96 ordination of actuation of the pMDI with inspiration of breath difficult (for example children and the
97 elderly) and for patients treated with inhaled glucocorticosteroids.

98 Any one specific spacing device may perform differently with different actives and similarly, any one
99 specific active in a specific pMDI may perform differently if inhaled through different spacing
100 devices. Therefore the ability to change from one spacing device to another or to use the same spacing
101 device with different pMDIs cannot be assumed. The development of a pMDI should always include
102 the testing of at least one specific named spacing device for use with the particular pMDI containing a
103 particular active. This spacing device has to be appropriate for the intended patient population.

104 The behaviour of the spacing device will depend on the volume and material of the holding chamber,
105 on the electrostatic properties of the internal surface of the chamber and on the way in which the
106 device is used. Hence the *in vitro* testing should be carried out by preparing the spacing device and
107 setting up the apparatus in a clinically relevant manner which may influence the performance of the
108 product, for example, inserting a time delay between actuation and inhalation to simulate tidal
109 breathing (if the dose is not evacuated in one breath) and washing/preparation of the spacing device
110 before and during use.

111 When all data collected in the development programme are based on the product administered via a
112 pMDI together with one or more specific, characterized spacing devices, the product can be authorised
113 subsequently for use **only** if used with the specific named spacing device(s).

114 If the product is to be administered with and without a spacing device, the use of the product alone as
115 well as the use of the product with the device must be supported by appropriate *in vitro* or *in vitro* and
116 clinical data (see sections 4.2 and 4.3 below). If these data are not in line with the criteria described in
117 section 4.3, below, clinical data covering the relevant patients groups (e.g. children, patients treated
118 with inhaled glucocorticosteroids) will be required in order to investigate the impact of the spacing
119 device on efficacy and safety.

120 If there are no specific recommendations for the use of a specific spacing device with the reference
121 product, the test product used both with and without a spacing device should be compared with the
122 reference product used without a spacing device; otherwise the reference product should be used in
123 accordance with the spacing device as stated in its own Summary of Product Characteristics (SPC).

124 If the spacing device is to be replaced subsequently by an alternative spacing device *in vitro*
125 characterisation of the new device may be sufficient to demonstrate comparability with the previous
126 device; however depending on the active substance this may not be appropriate and further clinical
127 development may be required (see sections 4.2 and 4.3, below).

128 The appropriately investigated spacing device(s) has to be specifically named in the SPC Section 4.2,
129 the package leaflet, any product promotional material and possibly also on the product labelling.

130 4.1.2 Dry powder inhalers

131 In contrast to the pMDI dry powder inhalers (DPIs) often show a high flow dependency in their
132 deposition characteristics. Therefore characterisation of flow rate dependency in the patient
133 populations in whom the DPI is to be used must be presented.

134 The dossier submitted has to include sufficient *in vitro* data such that the flow deposition
135 characteristics of the products within the range of clinically relevant pressure drops/flow limits can be
136 described.

137 Marketing authorisations for DPIs with a high flow rate dependency where pulmonary deposition and
138 subsequent systemic exposure may be much higher than is seen with inhalers with a low flow rate
139 dependency can only be granted for use in the patient populations studied in the clinical programme.
140 Extrapolation to patient populations other than those populations studied in the clinical programme is
141 not then appropriate and marketing authorisations will be restricted appropriately. For all DPIs the
142 patient population in whom the inhaler can be used should be carefully defined.

143 The use of a high flow rate dependent DPI as a reference product in a clinical study may raise issues in
144 respect of the conclusions which can be drawn regarding therapeutic equivalence unless deposition
145 characteristics and inspiratory flow rates are standardised. Therefore, equivalence should be assessed
146 across a range of inspiratory capacities (pressure drops/flow rates) which represent the patient
147 population covered by the authorisation for the reference product.

148 **4.1.3 Solutions and suspensions for nebulisation**

149 In specific circumstances (for example toddlers, the severely ill patient, the elderly, the disabled)
150 inhalation of medicinal products *via* a nebuliser, either a jet nebuliser or an ultrasonic nebuliser, is a
151 treatment option for patients with asthma and COPD. Generally nebulisers are sold separately from
152 solutions and suspensions containing active substances for nebulisation and therefore these
153 formulations are often inhaled via an available nebuliser rather than via the nebuliser used during the
154 development of the medicinal products for nebulisation itself.

155 However the differences in delivered aerosol between nebuliser systems currently available are
156 significant. Therefore a medicinal product formulated for nebulisation should be characterised using a
157 specified and standardized nebuliser system(s). Representative nebulisers for both jet and ultrasonic
158 nebuliser should be considered. The nebuliser system used should be described in the protocol in term
159 of:

- 160 • Nebuliser type
- 161 • Choice of driving gas
- 162 • Driving gas pressure
- 163 • Driving gas flow rate
- 164 • Nebuliser fill volume
- 165 • Time of nebulisation
- 166 • Residual solute volume
- 167 • Accessories

168 The nebuliser system studied in the development programme should be described in the SPC, package
169 leaflet and product literature and warnings should be included to state that the use of an alternative
170 nebuliser system may alter the pulmonary deposition of active substance and dose adjustment may
171 then become necessary.

172 Solutions for nebulisation with the same qualitative and quantitative composition as the authorised
173 reference product may be waived of any clinical study, with justification; however *in vitro* equivalence
174 must be demonstrated. For suspensions for nebulisation *in vitro* and clinical equivalence should be
175 demonstrated.

176 In non-pressurised, pump activated liquid reservoir metered dose inhalers the speed of plume is
177 decreased. In order to get a sufficient amount of active substance the patient has to inhale a specific
178 volume of the aerosol. In patients with a limited inhalational capacity (for example, children) it has to
179 be shown that the volume required to produce a clinical effect does not exceed the inhalational
180 capacity of the patient.

181 **4.1.4 Investigation of additional strengths**

182 Dose linearity in respect of pulmonary deposition should be investigated *in vitro* for both the test and
183 the reference product across all proposed strengths.

184 If dose linearity is demonstrated *in vitro* when different dose strengths of a known active substance are
185 sought it may be sufficient to establish therapeutic equivalence clinically with only one strength of the
186 active substance. It is usually appropriate to study the lowest strength, at more than one dose level, to
187 enhance the sensitivity of the study.

188 If linearity cannot be demonstrated with the reference product, either the test product has to be adapted
189 to the reference or therapeutic equivalence needs to be established with more than one strength of the
190 product.

191 If an additional strength of a product is to be developed the benefit/risk balance for the product must
192 remain acceptable.

193 The comparator should be the authorised innovator product if this product is still available. The choice
194 of comparator should be justified.

195 **4.2 PHARMACEUTICAL PROPERTIES AND THE NEED FOR A CLINICAL** 196 **PROGRAMME**

197 **4.2.1 New active substance**

198 Products containing a new active substance are required to undergo a full development programme
199 regardless of the type of device from which the new active substance is inhaled.

200 **4.2.2 Known active substance**

201 For abridged applications therapeutic equivalence to a reference medicinal product must be
202 substantiated. In some cases, the use of only comparative *in vitro* data, obtained with an accepted
203 method (e.g. multistage impactor/impinger), may be considered acceptable if the product satisfies **all**
204 of the following criteria (compared with the reference product):

- 205 • The product contains the same active substance (i.e. same salt, ester, etc.)
- 206 • The pharmaceutical dosage form is identical
- 207 • The active substance is in the solid state (powder, suspension): any differences in crystalline
208 structure and/or polymorphic form should not influence the solubility
- 209 • Any qualitative and/or quantitative differences in excipients should not influence the
210 performance of the product (e.g. delivered dose uniformity etc.), aerosol particle behaviour
211 (e.g. hygroscopic effect, plume dynamic and geometry) and/or the inhalation behaviour of the
212 patient (e.g. particle size distribution affecting mouth/throat feel or “cold Freon” effect)
- 213 • Any qualitative and/or quantitative differences in excipients should not change the safety
214 profile of the product
- 215 • The inhaled volume needed to get sufficient amount of active substance should be similar
- 216 • The instructions for use of the inhalation device are the same
- 217 • The inhalation device has the same resistance to airflow (within +/- 15%)
- 218 • The delivered dose is the same (within +/- 15% of labelled claim)

219 The complete individual stage particle size distribution profile should be provided. In case of flow rate
220 dependency, the comparative *in vitro* data should be obtained with a range of flow rates. This range
221 should be justified in relation to the intended patient population. The minimum (e.g. 10th percentile),
222 median and maximum (e.g. 90th percentile) achievable flow rate should be investigated.

223 The efficacy and safety of the medicinal product will depend on the amount of active substance that
224 reaches the lung and on the deposition site distribution. In addition, the safety will also be influenced
225 by the rate and extent of systemic absorption from the gastrointestinal tract (i.e. the swallowed
226 fraction). Therefore the *in vitro* comparison should be performed for the stages that represent the fine
227 particle mass as well as the upper stages of the impactor/impinger which are relevant to the efficacy
228 and safety of the medicinal product *in vivo*, unless otherwise justified.

229 The comparison should be performed per impactor stage or justified group of stages. At least 4 groups
230 of stages are expected. Justification should be based on the expected deposition sites in the lungs. The
231 maximum allowable *in vitro* difference should be indicated and justified, e.g. +/- 15% may be
232 justifiable. Per impactor stage or justified group of stages the 90% confidence intervals for the
233 observed *in vitro* differences must be calculated. Based on the pre-established maximum allowable
234 differences, a decision regarding equivalence can be made. The only exemption might be medicinal
235 products for nebulisation (see also section 4.1.3).

236 If **any of** the above-mentioned criteria are not fulfilled or when equivalence cannot be demonstrated
237 on the basis of the *in vitro* comparison, *in vivo* studies should be performed to substantiate
238 equivalence.

239 4.3 CLINICAL DEVELOPMENT

240 4.3.1 Determination of pulmonary deposition

241 Pulmonary deposition studies investigate the extent and pattern of pulmonary deposition of an inhaled
242 active substance.

243 Different excipients, different devices or different pharmaceutical quality of inhalation products
244 containing the same active substance may have an important influence on pulmonary deposition
245 resulting in a clinically relevant impact on efficacy and safety. If the product for which a new
246 marketing authorisation is sought fails to show equivalence to the reference product based on *in vitro*
247 data (see section 4.2.2 above), one way to demonstrate equivalence in terms of local availability may
248 be through a comparison of pulmonary deposition.

249 Pulmonary deposition studies are designed as double blind, crossover studies and should be carried out
250 using a clinically relevant dose(s) and strength(s) of the product (which may be determined from the *in*
251 *vitro* data). These studies can be performed in healthy volunteers.

252 Pulmonary deposition can be investigated by conducting imaging or pharmacokinetic studies.

253 Pharmacokinetic studies may have some advantages, even though they provide data indirectly from
254 plasma or urine: Pharmacokinetic studies are easier to perform, they are safer due to the lack of
255 radiation, they avoid the risk of altering the formulation during radio-labelling, they can demonstrate
256 linear dose-response relationships more easily, they measure total systemic exposure and can separate
257 pulmonary from gastrointestinal absorption and they do not take into account active substance
258 removed by mucociliary clearance. Limitations with pharmacokinetic studies include their inability to
259 differentiate the distribution of drug within the different zones of the lung following inhalation and in
260 some cases plasma concentrations are not measurable at clinical doses or are near the lower limit of
261 quantification such that results may be highly variable.

262 Equivalent pulmonary deposition in combination with safety data (for example data from a systemic
263 safety PK study) **might** be considered as sufficient demonstration of therapeutic equivalence.
264 Otherwise therapeutic equivalence must be demonstrated by means of appropriate clinical studies.

265 Pulmonary deposition (whenever possible) and *in vitro* characterisation of the active drug, comparing
266 the new product with a reference product, should be investigated prior to carrying out therapeutic
267 equivalence studies.

268 4.3.1.1 Imaging studies

269 Regional quantification of the pulmonary deposition of two products can be carried out by measuring
270 radioactivity in the different segments of the lung. Two- or three-dimensional scintigraphic methods
271 can be used. Equivalent lung deposition of two drugs can be concluded if the 95 % CI of the
272 radioactivity in all of the several airway areas is within a range of 0.8 to 1.25. The whole lung
273 percentage deposition of the drug should be measured as well as the proportion deposited in the
274 central, intermediate and peripheral lung zone, oropharynx, mouthpiece, actuator and exhalation filter.
275 It has to be assured that the radio-labelling of the inhaled products has no influence on the deposition
276 characteristics.

277 4.3.1.2 Pharmacokinetic studies

278 A pharmacokinetic study designed to assess pulmonary deposition, has to be able to exclude
279 absorption of the active moiety from the gastrointestinal tract (for example by using charcoal
280 blockade); a pharmacokinetic study to investigate systemic safety has to measure total systemic
281 exposure and therefore must not exclude that amount of the active moiety absorbed through the
282 gastrointestinal tract. In accordance with the standard accepted methods of assessment of
283 bioequivalence C_{max} , the time to C_{max} (T_{max}) and the area under the curve (AUC) should be compared.
284 Equivalent pulmonary deposition of two inhaled products may be concluded if the 95 % confidence
285 interval for each parameter lies within the acceptance range of 0.8 to 1.25.

286 4.3.2 Pharmacodynamic studies

287 4.3.2.1 General considerations in the investigation of therapeutic equivalence

288 Therapeutic equivalence is defined as equivalent efficacy and safety when the new inhaled product for
289 which a marketing authorisation is sought is compared with an appropriate reference product.
290 Therapeutic equivalence demonstrated by means of appropriate clinical studies using well-validated
291 study designs and comparing the test product with the reference product, will almost always be
292 required and becomes mandatory when equivalence is not shown *in vitro* and is not shown through
293 investigation of pulmonary deposition.

294 Based on different inhalation techniques required for different inhalation devices it is recommended
295 that the test and reference product should be inhaled from the same kind of device (for example both
296 the test and the reference product should be administered via a pMDI or both should be administered
297 via a DPI) wherever possible, when assessing therapeutic equivalence.

298 If clinical studies are needed and the reference product has an authorised indication which includes
299 both asthma and COPD, therapeutic equivalence studies may only be needed in one of the patient
300 populations in order to obtain a marketing authorisation. Generally such studies are easier to carry out
301 in patients with asthma. However if therapeutic equivalence to the reference product is demonstrated
302 (in respect of both efficacy and safety) in one clinical indication, say asthma, comparative *in vitro* data
303 must be provided to demonstrate that the test and reference product produce comparable fine particle
304 performance through the flow rate and pressure drop range which are clinically applicable to **all**
305 patients in whom the test product will be used, in order that a marketing authorisation can be granted
306 which will include all therapeutic indications as listed for the reference product.

307 4.3.2.2 Requirements for clinical studies in patients with asthma

308 Two different types of pharmacodynamic study provide acceptable methods for investigating
309 therapeutic equivalence of inhaled drugs – studies of bronchodilatation and studies of
310 bronchoprotection. Depending on therapeutic class one or other or both of these types of study may be
311 used to satisfy the requirements of comparative efficacy.

312 Independent of the type of study, either bronchodilatation or bronchoprotection, the trial should be
313 carried out in patients with asthma and who demonstrate reversibility of airway function, as assessed
314 by measurement of forced expiratory volume in one second (FEV₁), of $\geq 15\%$, or $\geq 12\%$ and a 200 ml
315 improvement in FEV₁, 15 minutes after inhalation of an appropriate inhaled short-acting β_2 adrenergic
316 agonist (SABA).

317 The study carried out must be sensitive enough to be able to discriminate between the two comparator
318 products and to be able to pick up differences which might exist between the two products. Relative
319 potency is considered a sensitive way of detecting differences between products and therefore is
320 recommended. Demonstration of therapeutic equivalence on the y-axis could also be acceptable
321 providing that the assay sensitivity is demonstrated indisputably. To enhance assay sensitivity it is
322 recommended that the following be considered:

- 323 • Inclusion of less than optimally controlled symptomatic asthmatic patients (according to
324 GINA Guidelines 2006) in studies of bronchodilatation.
- 325 • In general and unless otherwise justified, demonstration of assay sensitivity will require
326 testing more than one dose of both the test and the reference products.
- 327 • Use of doses at the lower end of the recommended dose range (on the steep part of the
328 dose-response curve).

329 Patients recruited to the study should be able to demonstrate a clinically relevant response to
330 treatment.

331 Therapeutic equivalence in respect of safety should be demonstrated by investigation of
332 bioequivalence based on pharmacokinetic data, relevant cardiovascular, biochemical and physiological
333 parameters, and monitoring of adverse events. The highest recommended dose has to be administered
334 when assessing safety. However safety analyses should be included in the efficacy studies regardless
335 of the dose being studied whenever possible. The duration of a safety study depends on the therapeutic
336 class of the test/active substance.

337 Two products will be considered as equivalent if the following criteria are completely fulfilled:

338 - **Efficacy:** If the relative potency approach is used the 95% confidence interval for the primary
339 endpoint must be contained entirely within 80 – 125 %.

340 - **Safety:** If possible bioequivalence in respect of systemic exposure should be demonstrated
341 (the 90% confidence interval must be contained entirely within 80 – 125%). Otherwise
342 equivalence in respect of relevant pharmacodynamic safety variables needs to be
343 demonstrated. Also there should be no evidence that the test product is worse than the
344 reference product in respect of changes in vital signs, biochemical parameters, frequency of
345 adverse events.

346 4.3.2.2.1 Bronchodilatation studies

347 Equivalent therapeutic efficacy can be investigated by measurement of the bronchodilating effect of
348 the test and the reference product through appropriate primary and secondary endpoints. The duration
349 of the study and the choice of primary and secondary endpoints are dependant on the therapeutic class
350 of the test product. Overall sensitivity of the study can be increased by the inclusion of stable, but less
351 than optimally controlled or only partially controlled patients with asthma. Less than optimally
352 controlled asthma is defined according to pulmonary function, level of symptoms including nocturnal
353 symptoms and nocturnal awakening, daily activity and/or daily requirement of *reliever* medication, at
354 baseline (measured during a run-in period). The study design should incorporate at least two dose
355 levels.

356 4.3.2.2.2 Bronchoprotection studies

357 The bronchoprotective potency of a drug to provide protection against hyperresponsiveness can be
358 assessed through bronchoprotection studies, either direct provocation for example with methacholine,
359 histamine, acetylcholine or indirect provocation with adenosine monophosphate (AMP) or mannitol.

360 Bronchoprotection studies require a high degree of standardisation (for example choice of
361 provocation, aerosol generation, nebuliser output, inhalation procedure, physical aspects, exclusion of
362 diurnal variation, etc). It is recommended that the ATS Guideline be considered in this regard.
363 Generally a double blind, double dummy, crossover study design is recommended. The primary
364 outcome variable, the provocative concentration or provocative dose of the provocation agent which
365 produces a 20% fall in FEV₁ (PC₂₀FEV₁ or PD₂₀FEV₁) must be measured at the time of the expected
366 maximum effect of the drug. At least two dose levels should be studied.

367 The use of bronchial challenge as a means of assessing therapeutic equivalence will depend on the
368 therapeutic class of the test product.

369 4.3.2.3 Therapeutic class - specific considerations in the investigation of therapeutic equivalence

370 4.3.2.3.1 Bronchodilators

371 Inhaled bronchodilators fall into three categories - short-acting β_2 adrenoceptor agonists (SABAs),
372 long-acting β_2 adrenoceptor agonists (LABAs) and anticholinergics.

373 Short-acting β_2 adrenoceptor agonists

374 For the SABA either a single dose bronchodilatation study or a bronchial challenge study are
375 acceptable study designs for the assessment of therapeutic equivalence. In the bronchodilatation model
376 an appropriate primary variable will be the FEV₁AUC; in the bronchial challenge study the primary
377 variable will be either the PC₂₀FEV₁ or PD₂₀FEV₁ (see 4.3.2.2.2, above).

378 In these therapeutic equivalence studies the safety of SABAs should be investigated through
379 bioequivalence based on pharmacokinetic data following administration of a single dose and also
380 through documentation of adverse events and vital signs, assessment of any evidence of paradoxical
381 bronchospasm and recording of laboratory parameters. If conclusions cannot be drawn from such
382 investigations cumulative dose clinical studies may also be used in the assessment of safety.

383 Long-acting β_2 adrenoceptor agonists

384 Initial requirements in the assessment of therapeutic equivalence in respect of efficacy of LABAs are
385 the single dose comparative studies of either bronchodilatation or bronchoprotection as for the

386 SABAs. However the onset of action (defined as a FEV₁ increase of 15%, or 12% and 200 ml, from
387 baseline), the maximum response and the longer duration of effect of the LABA must be taken into
388 consideration in the design of the study. In the bronchodilatation model the primary variable will be
389 the FEV₁AUC; in the bronchial challenge study the primary variable will be either the PC₂₀FEV₁ or
390 PD₂₀FEV₁.

391 An appropriate washout time between treatments has to be defined in any crossover design and
392 justified in the protocol. Baseline measurements prior to each treatment period have to be documented
393 to assess any possible carry-over effect.

394 The dose range should be explored in the single dose studies with assessment of low and high doses to
395 enable demonstration of dose-response.

396 Safety of LABAs should be investigated through bioequivalence based on pharmacokinetic data and
397 by measurement of biochemical parameters (including measurements of serum potassium and plasma
398 glucose), recording of adverse events, vital signs and serial ECGs and measurement of the QTc
399 interval, and assessment of any paradoxical bronchospasm. The safety profile must be defined for the
400 maximum recommended dose regimen.

401 **Anticholinergic drugs**

402 The investigation of therapeutic equivalence in respect of anticholinergic drugs is similar to that of
403 SABAs and LABAs. However the differing characteristics of the β₂ agonists and the anticholinergic
404 drugs have to be taken into account particularly in respect of onset of action and duration of effect. In
405 any bronchial challenge study the preferred provocation agent would be methacholine.

406 **4.3.2.3.2 Inhaled glucocorticosteroids**

407 The demonstration of therapeutic equivalence of inhaled glucocorticosteroids (ICS) is difficult. A
408 successful therapeutic equivalence study requires demonstration of a significant dose-response
409 relationship with the study of at least two doses of the test compared with, if possible, two doses of the
410 reference product. There are certain circumstances when the use of excessive multiple actuations are
411 required to achieve the required dose. This may result in unacceptable impact on the patient/volunteer
412 (e.g. high powder loading of the excipient from a DPI). The use of a different higher strength product
413 may be justified in such circumstances. Comprehensive *in vitro* dose proportionality from the different
414 strength products should be fully demonstrated.

415 Currently the most well-used study design is the double blind, randomised, parallel group comparison
416 of the test and the reference product; if the chosen study design differs from this, the reasons for doing
417 so must be justified by the Applicant.

418 An alternative is the crossover study, a study design which has the advantages of the ability to study a
419 much smaller population and the ability to detect within-subject variability; however concerns
420 regarding an unequal carry-over of corticosteroid effects within subjects between treatment periods
421 and the potential difference in the baselines at the beginning of the two treatment periods may
422 outweigh the advantages unless the impact of any carry-over effect can be controlled. Carry-over
423 effects between treatment periods must be at least equal.

424 Patients recruited should have demonstrable room for improvement in pulmonary function to respond
425 differently to the two doses of the inhaled corticosteroid and should be symptomatic (see section
426 4.3.2.2.1). The population included should be as homogeneous as possible to decrease variability and
427 increase the power to detect a significant dose-response relationship and obtain an estimate of the
428 difference between formulations in respect of pulmonary function with a sufficiently narrow
429 confidence interval. However the population should also be the target population.

430 The primary efficacy variable should be a pulmonary function measure and preferably FEV₁ measured
431 regularly, if possible daily at home or at least every two weeks in the clinic. [Regular measurement of
432 FEV₁ is a more sensitive measure of pulmonary function than peak expiratory flow rate (PEFR) which
433 should be recorded daily at home as a secondary efficacy variable]. Electronic diary cards should be
434 used if at all possible. Symptom scores, frequency of use of *reliever/rescue* medication and
435 exacerbations should be recorded as secondary endpoints. Other efficacy variables which may be
436 considered include PC₂₀, PD₂₀, expired nitric oxide (eNO), sputum eosinophils. Whatever primary
437 efficacy variable is chosen should be justified based on its sensitivity to detect differences between

438 adjacent doses of the inhaled corticosteroid. The duration of treatment periods should be at least eight
439 (if not twelve) weeks, any shorter treatment period should be justified.

440 Equivalent safety or an improved safety profile must be demonstrated. Appropriate safety monitoring
441 within the therapeutic efficacy studies would include the recording of local adverse effects and any
442 evidence of paradoxical bronchospasm and the assessment of systemic effects.

443 In addition, specific safety investigations must be carried out following inhalation of the maximum
444 recommended daily dose of the ICS regularly over time in both adults and children. If possible
445 systemic safety should be demonstrated through pharmacokinetic bioequivalence and measurement of
446 pharmacodynamic parameters in adults and children.

447 The current view in respect of the measurement of systemic effects of ICSs is to assess the effect on
448 the hypothalamic pituitary adrenocortical (HPA) axis in adults and on the HPA axis and/or on lower
449 leg bone growth rate in children. Knemometry is validated, accurate and reproducible and has been
450 used previously in the early assessment of systemic safety of ICSs in children.

451 In assessing the HPA axis in adult patients one option is the 24-hour urinary-free cortisol, if possible
452 coupled with repeated measures of plasma cortisol over 24 hours. Such assessments should be made at
453 least at the beginning and end of the eight- (or twelve-) week study.

454 A second and more robust alternative in adult patients, the repeated assessment of the change from
455 baseline in 24-hour plasma cortisol as measured by AUC as the primary variable coupled with the
456 change from baseline in 24-hour urinary-free cortisol as a secondary variable is an acceptable way to
457 assess systemic effects of the ICSs.

458 A further alternative method of assessment of systemic effects on the HPA axis in adults, and an even
459 more robust assessment and a more preferred assessment, is the study of a population of normal
460 healthy volunteers with evaluation of HPA axis function using the ACTH (Synacthen) short
461 stimulation test. Such a study would require treatment of healthy volunteers with a total daily dose of
462 ICS at the upper limit of the proposed dose range over a treatment period of at least four weeks. The
463 measurement of plasma cortisol over 24 hours at intervals during the study could be incorporated into
464 this type of study.

465 Generally it is not felt to be appropriate to subject children to repeated venopuncture and therefore
466 pharmacokinetic studies and the repeated measurement of plasma cortisol have not been used as first
467 line methods to assess the systemic burden of ICSs in this young age group. However in the light of
468 the very real need to ensure the systemic safety of these drugs in children and the acceptance that other
469 methods to assess the systemic load are far from robust or even satisfactory, the use of an indwelling
470 cannula to enable the collection of blood samples to measure both blood levels of the drug and any
471 active metabolites and plasma cortisol at intervals over time should be considered. This approach may
472 represent the best way of collecting reliable information on comparative systemic safety in children
473 with asthma treated with ICSs. The ACTH short stimulation test is not recommended and should not
474 be used for the assessment of the systemic effects of ICSs in children [Further discussion on the
475 requirements for therapeutic equivalence studies in children will be addressed in appendix 1 (public
476 consultation expected Q1 2008) – see section 4.6].

477 Whatever methods of assessing systemic effects of ICSs are used they should be fully discussed and
478 justified in the dossier submitted. Advice from appropriate experts in the field might be useful to
479 ensure that tests and assessments carried out are appropriate and are in line with current thinking.

480 **4.3.2.3.3 Combination products**

481 For fixed combination products of known active substance therapeutic equivalence should be
482 demonstrated for each/all of the component actives of a fixed-dose combination product and study
483 design will depend on the specific actives in the combination, for example, efficacy and safety of the
484 combination of an ICS and a LABA might be investigated in one study in which outcome measures
485 capable of assessing both active components in the combination separately are included (co-primary
486 variables in respect of efficacy will need to be defined, one for each component of the combination).
487 The study design should include two doses of each combination product (the test and the reference
488 combination product) in order to show a significant statistical dose-response relationship.

489 Furthermore establishing therapeutic equivalence for combinations of ICSs and LABAs might be
490 through separate studies assessing each separate active. The efficacy of the LABA component can be
491 assessed following inhalation of a single dose through either measurement of bronchodilatation over at
492 least 80% of the duration of action or bronchial challenge studies; the efficacy of the ICS component
493 will be through the study of multiple dose inhalations over time – see sections 4.3.2.3.1 and 4.3.2.3.2,
494 above.

495 For new fixed combination products with no approved fixed combination reference product the
496 inclusion of an additional treatment arm in which patients would receive the ICS component alone is
497 necessary with further reference to the *CPMP Note for Guidance on Fixed Combination Medicinal
498 Products CPMP/EWP/240/95*. The ICS alone treatment group could receive the same dose of
499 corticosteroid as in the combination product or alternatively receive a higher dose, although care
500 should be taken to ensure that patients are not then over-treated.

501 The assessment of the safety of combination products is as for the single actives and as described
502 above in sections 4.3.2.3.1 and 4.3.2.3.2.

503 **4.3.2.3.4 Sodium cromoglycate and nedocromil sodium**

504 For sodium cromoglycate and nedocromil sodium therapeutic equivalence in terms of efficacy and
505 safety can be obtained from bronchial challenge studies.

506 **4.4 CLINICAL TRIALS AND CHANGE OF PHARMACEUTICAL SPECIFICATIONS**

507 Pharmaceutical drug product specifications should be set based on pharmaceutical results of the
508 batches used in the clinical studies. Any changes to these specifications (for example, fine particle
509 dose) should also be based on data supported by clinical batches.

510 A widening of the specifications cannot be supported at a later date, when therapeutic equivalence has
511 been demonstrated following the completion of appropriate clinical studies, without possibly affecting
512 the conclusions drawn from the original clinical programme.

513 **4.5 CHRONIC OBSTRUCTIVE PULMONARY DISEASE**

514 See section 4.3.2.1, above.

515 If clinical studies are carried out in patients with COPD the study proposals discussed above may not
516 be appropriate. The *CPMP Points to Consider on Clinical Investigation of Medicinal Products in the
517 Chronic Treatment of Patients with Chronic Obstructive Pulmonary Disease (COPD)
518 CPMP/EWP/562/98* should be considered.

519 **4.6 CHILDREN**

520 See appendix 1 (public consultation expected Q1 2008).

521 **4.7 SAFETY OF NEW EXCIPIENTS**

522 The safety profiles of active drug substances as currently formulated are not in question. However,
523 potential safety concerns do arise, both from the use of new excipients where safety in man following
524 inhalation has not been investigated previously, and also from any possible interactions between these
525 new excipients and the active drug substances, interactions that might enhance toxicity of the active
526 drug substance. A change in excipients might result in changes in drug deposition patterns within the
527 lung which might affect absorption and systemic safety. Full animal toxicology will have been
528 completed for each new excipient but such data will not remove the need for clinical safety studies in
529 man.

530 The aims of a safety programme in this situation are two fold:

- 531 i) to determine the safety of a new excipient mix in a formulated medicinal product
- 532 ii) to assess interactions which may occur between an active drug substance and an excipient mix
533 which might result in changes in the safety of the medicinal product.

534 The assessment of a new excipient mix need only be addressed once, but the assessment of
535 interactions will be required for each drug substance combined with that new excipient mix.
536 Obviously if changes in absorption or systemic safety are seen in these interaction studies, these

537 changes will need to be quantified and long-term safety assessments of the active drug formulated in
538 that excipient mix may be required.

539 A change in excipient mix will necessitate further long-term safety assessment.

540 **DEFINITIONS**

541 Dose Amount of drug administered at single occasion

542 Delivered/Emitted Dose Dose released at the mouthpiece of the device

543 Linearity In this context a function of $f(x)=ax+b$, with $a=1$ and $b=0$ is not
544 necessary.

545 Metered Dose Dose released from the valve

546 Relative Potency The relative potency of the test product to the reference product is
547 defined as the dose of the test product that produces the same
548 biological response as one unit of the dose of the reference product

549 Spacing device Also called a holding chamber

550 Strength/dose Strength is what is metered in the device for a single inhalation
551 manoeuvre whereas a single dose may contain for example 2 puffs of
552 a pMDI or 4 puffs of a pMDI. So, for doses of 12 and 24 μg
553 formoterol pMDI one and 2 puffs of the 12 μg strength or two puffs
554 of both the 6 μg and 12 μg strength might be used.

555 Pulmonary Deposition Amount of active substance deposited in the airways (mouth and
556 throat excluded)