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4 **Guideline on quality of oral modified release products**
5 **Draft**

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6
7 This guideline together with the Guideline on Quality of Transdermal Patches replaces Note for Guidance
8 on Modified Release products: A: Oral dosage Forms B: Transdermal Dosage Forms. Part I (Quality).

9
10 Comments should be provided using this [template](#). The completed comments form should be sent to qwp@ema.europa.eu

Keyword	Oral dosage form, modified release
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11 **Guideline on quality of oral modified release products**

12 **Table of contents**

13 **1. Introduction 3**

14 1.1. Preamble 3

15 1.2. Scope 3

16 **2. Prolonged release oral dosage forms 3**

17 2.1. Development pharmaceuticals..... 3

18 2.1.1. General remarks 3

19 2.1.2. Therapeutic objectives and principle of the release system 4

20 2.1.3. Development of dissolution methods 4

21 2.1.4. Discriminatory power of the dissolution test 6

22 2.1.5. Bioavailability study 6

23 2.1.6. Comparison of dissolution profiles 6

24 2.1.7. *In vitro-in vivo* comparison 7

25 2.2. Setting specifications 8

26 2.3. Control strategy 9

27 2.4. Variations to products 9

28 **3. Delayed release dosage forms 9**

29 3.1. Development pharmaceuticals..... 10

30 3.2. Setting specifications 10

31 3.3. Control Strategy 11

32 3.3. Variations to products 11

33 **Annex 1 12**

34 **Annex 2 15**

35 **1. Introduction**

36 **1.1. Preamble**

37 Pharmaceutical dosage forms may be developed in which the rate and/or place of release of active
38 substance(s) has in some way been modified compared with conventional release formulations. Such
39 modifications may have a number of objectives, such as maintaining therapeutic activity for an extended
40 time, reducing toxic effects, protecting the active substance against degradation due to low pH, targeting
41 the active substance to a predefined segment of the gastrointestinal tract for local treatment or targeting
42 active substance release at specified time-points.

43 This section I document covers the various parts of the application for Marketing Authorization related to
44 quality and should be read in conjunction with section II of this NfG relating to clinical aspects.
45 Furthermore, it is clear that this NfG cross-references to other quality guidelines and to official
46 compendia.

47 For clear definitions on the terminology used to describe different types of release models and other
48 definitions, reference is made to Annex I.

49 **1.2. Scope**

50 This NfG concerns quality aspects, especially pharmaceutical development and *in vitro* testing, of dosage
51 forms in which the release of active substance is modified. This guideline only covers delayed release oral
52 dosage forms with the principle of gastro-resistance and prolonged release oral dosage forms. Pulsatile
53 and accelerated release dosage forms are not covered by the current guideline. Delayed release dosage
54 forms with other principles, including those designed to release in a specific area of the gastrointestinal
55 tract in response to a specific trigger (e.g. enzymes) or at specific time(s) after ingestion are not
56 specifically addressed.

57 Many principles discussed under paragraph 2 with respect to prolonged release oral dosage forms will be
58 relevant to other modified release dosage forms intended for oral administration or via other routes.

59 **2. Prolonged release oral dosage forms**

60 **2.1. Development pharmaceuticals**

61 **2.1.1. General remarks**

62 The quality of a prolonged release dosage form is continuously improved during the development of a new
63 drug product. The choice of the composition is normally made early in the development based on
64 small-scale batches and takes into account physicochemical properties of the drug substance, stability
65 and drug absorption characteristics throughout the gastrointestinal tract. As soon as the constituents are
66 chosen, gradual scaling up of the manufacturing process will start. During this period it is reasonable to
67 expect that adjustments will be necessary to reach full-scale production. These adjustments might be
68 changes in composition, manufacturing processes, equipment or manufacturing site.

69 In some cases these adjustments may have an effect on the properties of the drug product. It is therefore
70 recommended that an *in vitro* dissolution test is developed which is able to detect changes which may
71 have an effect on the efficacy or safety of the product.

72 Pharmaceutical development should establish the link from pharmacokinetic parameters through *in vivo*
73 drug release to *in vitro* dissolution rate.

74 The formulation chosen in early development should be tested under different dissolution conditions to
75 determine its sensitivity/robustness to the expected physiological environment after administration. The
76 discriminatory power of the test conditions chosen for routine control may be determined by comparison
77 of the *in vitro* dissolution data and the bioavailability data of the different formulations. If a Level A *in*
78 *vivo-in vitro* correlation (IVIVC) is established, the dissolution test - after proper validation - can be used
79 as a qualifying control method with *in vivo* relevance, while in the absence of a Level A IVIVC the
80 dissolution test can be used only as a quality control method.

81 After completed scale-up it is reasonable to compare the laboratory/pilot scale batches with the full
82 production scale batches in a bioavailability study if the scale-up factor exceeds 10 (compared to the
83 laboratory/pilot scale biobatch) in order to verify that the dissolution test conditions chosen are
84 appropriate for the release of clinical materials, scale-up and manufacture (see also 2.1.3. and 2.1.4 and
85 2.1.5).

86 **2.1.2. Therapeutic objectives and principle of the release system**

87 The therapeutic objectives and rationale of the prolonged release product should be provided.
88 Pharmacokinetic (e.g. AUC, C_{max} , T_{max} , $t_{1/2}$) and physico-chemical characteristics of the active substance
89 (e.g. solubility at different pH, partition coefficient, particle size, polymorphism) relevant to the
90 development of the product should be given. Detailed information on the release controlling excipient(s)
91 should be given. Reference is made to the guidelines on pharmaceutical development.

92 The following characteristics of the prolonged release system should be described:

- 93 • the manner in which prolonged release is intended to be achieved (membrane type, matrix, etc.);
- 94 • the release mechanism and kinetics (diffusion, erosion, osmosis, etc. or a combination of these);
- 95 • the system format e.g. single non-disintegrating unit, disintegrating tablet/capsule containing
96 multiple-units of pellets, etc.

97 It should be demonstrated that the prolonged release product maintains its drug release characteristics
98 regardless of relevant variability in physiological conditions. Examples of such variability include gastric
99 and intestinal transit time, food effect, pathological gastrointestinal fluid composition and concurrent
100 alcoholic intake, if and where relevant.

101 In general, prolonged release oral dosage forms should not have a score line because subdivision or other
102 manipulation of modified release products may adversely affect the modified release properties of the
103 dosage form, possibly leading to dose dumping. Any recommendation on subdivision of a modified release
104 dosage form should be supported by scientific justification that the subdivision does not affect the
105 modified release characteristics, including *in vitro* and/or *in vivo* data as appropriate.

106 **2.1.3. Development of dissolution methods**

107 The release rate should be tested *in vitro* by a dissolution test method. The development of a suitable
108 dissolution test method should be based on the physicochemical *in vitro* and *in vivo* characteristics of the
109 active ingredient and the drug product considering the mechanism of release.

110 This *in vitro* dissolution test must be capable of:

- 111 • discriminating between batches with respect to critical manufacturing variables which may have an
112 impact on the desired bioavailability;

- 113 • testing for batch to batch consistency of pivotal clinical, bioavailability and routine production batches;
114 • determining stability of the relevant release characteristics of the product over the proposed shelf life
115 and storage conditions.

116 The prolonged release formulation should therefore be tested *in vitro* under various conditions (media, pH
117 (normally pH range 1-7.5; in cases where it is considered necessary pH 1-8), apparatus, agitation, etc.).
118 Testing conditions, including sampling timepoints and frequency providing the most suitable
119 discrimination should be chosen.

120 If media with a low buffering capacity are used, the pH should be controlled during the dissolution test to
121 be sure that there is no influence of dissolved active ingredient and/or excipients on the dissolution
122 conditions during the test period.

123 If a surfactant is used in the dissolution medium, the amount needed should be justified. The choice of the
124 surfactant should be discussed and its consistent batch to batch quality should be ensured.

125 The inclusion of enzymes in the media is acceptable, and even encouraged, when justified (e.g., colonic
126 delivery). If enzymes are added to the dissolution media, a rationale should be given for the type and
127 concentration of enzymes added. Further, consistency of the batch to batch quality of the enzymes should
128 be ensured including activity (IU/mg or IU/ml) or concentration (mg/ml) as appropriate. Note that the
129 enzyme concentration of the SGF / SIF media prescribed in the Ph.Eur. are much higher than
130 physiologically relevant values.

131 Justified enzyme concentrations should be used when the enzymes constitute part of the dissolution
132 control mechanism. The use of biorelevant media may improve the correlation to *in vivo* data and may
133 detect a potential food effect.

134 The volume of medium should preferably ensure sink conditions.

135 For formulations having a zero order release kinetics (with or without lag time) a specification of the
136 dissolution rate over time (per cent of label claim per hour) for a given interval may be suitable instead of
137 the cumulative amount dissolved at a given time point (see also section 2.2). For this type of product, a
138 graphical presentation of the dissolution rate versus time should be additionally presented in order to
139 justify that the product can be regarded as a zero-order release formulation. For additional details with
140 respect to the choice of apparatus, testing conditions, validation/qualification and acceptance criteria,
141 reference is made to the Ph. Eur.

142 Special attention should be paid to the importance of any variation in the active substance (e.g. particle
143 size, polymorphism), release controlling excipient(s) (e.g. particle size, gelling properties) or
144 manufacturing process.

145 The assay method of the active ingredient in dissolution samples should be validated according to the
146 relevant ICH guidelines "Validation of analytical procedures" and "Validation of analytical procedures:
147 Methodology", with special attention to the stability of the active ingredient dissolved in the medium and
148 effects from the excipients.

149 Identical or, if not possible, comparable test conditions should be used for different strengths of the same
150 product.

151 Normally in development, individual dosage unit results, the mean value and a measure of variability
152 (e.g. standard deviation or 95 % confidence interval) should be presented at each time point. Use of other
153 statistical approaches must be justified. Dissolution profiles should be determined for all strengths and, if
154 relevant, for any changes in the composition and/or manufacturing process of the product during
155 development.

156 **2.1.4. Discriminatory power of the dissolution test**

157 It should be shown that the dissolution test under the chosen test conditions is able to discriminate
158 between batches with acceptable and non acceptable *in vivo* behavior.

159 Showing discriminatory power may be achieved in one of the following approaches in order of priority:

- 160 • It is best practice to include batches which have failed to show acceptable pharmacokinetic parameters
161 *in vivo*. Based on the dissolution results, meaningful specifications may be set to reject such batches
162 due to their dissolution data. This may be supported quantitatively through a validated IVIVC, which
163 has been developed under consideration of batches with unacceptable pharmacokinetic parameters;
- 164 • In cases where there are no non-acceptable batches available, the dissolution data may be compared
165 to the average results of the pharmacokinetic parameter (point estimates) of the *in vivo* studies. These
166 data may be compared by checking the rank order of the results;
- 167 • If neither of the first two approaches is feasible, the discriminatory power may be shown by
168 deliberately varying an attribute of the active ingredient (e.g. particle size distribution), composition
169 and/or manufacturing process parameters, in order to produce different *in vitro* dissolution behavior,
170 without generating *in vivo* data for these batches. However such test procedures may lead to
171 over-discrimination, i.e. even batches with acceptable *in vivo* performance may be rejected by the
172 quality control method.

173 **2.1.5. Bioavailability study**

174 A summary of the bioavailability studies should be given. The data should include information on
175 pharmacokinetics ($AUC_{0 \rightarrow t(\text{last})}$, $AUC_{0 \rightarrow \infty}$, C_{max} , and other relevant parameters; for generic products
176 also the point estimates and 90% confidence intervals), manufacturing sites and dates, batch sizes and
177 numbers, formulations and dissolution results of the batches used.

178 Bioavailability studies should be performed with batches of 100,000 units or at least 10% of full
179 production scale, whichever is greater, unless pivotal clinical studies have been performed with batches of
180 this size. In this case bioavailability studies performed with batches of a smaller scale may be sufficient if
181 these batches have been produced in a manner representative of the full scale manufacturing process.
182 So, for example, if phase II trials (including PK/BA-studies) are conducted at a scale of 15 kg, the pivotal
183 clinical trials (no BA data available) at a scale of 60 kg and full production scale is intended to be 600 kg,
184 no additional BA-studies at a scale of 60 kg are required.

185 **2.1.6. Comparison of dissolution profiles**

186 On several occasions dissolution profiles have to be compared for similarity, e.g. after scale-up or
187 changes in composition and/or manufacturing process or in case of a biowaiver for different strengths.
188 Similarity of dissolution profiles should be established with at least 12 individual values per time point.
189 Consideration should be given to the sampling timepoints and frequency, taking into account the
190 physicochemical *in vitro* and *in vivo* characteristics of the active ingredient and the mechanism of release
191 of the drug product.

192 In cases where the biowaiver is to be applied for approval of different strengths, if not all strengths of a
193 test drug product are compared *in vivo* versus the reference, the dissolution of the other strengths of the
194 test product will be compared to the strength of the test product used in the bioequivalence study.

195 The profiles should be compared and their similarity may also need to be demonstrated by statistically
196 justified methods using model-independent or model-dependent methods e.g. linear regression of the

197 percentage dissolved at specified time points, statistical comparison of the parameters of the Weibull
198 function or calculation of a similarity factor.

199 **2.1.7. *In vitro-in vivo* comparison**

200 *In vitro* dissolution testing is not only important as a necessary quality assurance for batch-to-batch
201 consistency but also to indicate consistency within a batch (i.e. that individual dosage units will have the
202 desired *in vivo* performance). By establishing a meaningful correlation between *in vitro* release
203 characteristics and *in vivo* bioavailability parameters, the *in vitro* dissolution test can serve as a surrogate
204 marker for *in vivo* behaviour and thereby confirm consistent therapeutic performance of batches from
205 routine production. The variability of the data should be reported and discussed when establishing a
206 correlation. In general the higher the variability in the data used to generate the *in vitro-in vivo*
207 correlation (IVIVC), the less confidence can be placed on the predictive power of the correlation.

208 An established Level A IVIVC may reduce the number of *in vivo* studies during product development, be
209 helpful in setting specifications and be used to facilitate certain regulatory decisions (e.g. scale-up and
210 post-approval variations). Therefore, an attempt to develop such an IVIVC should be considered by the
211 applicant. Furthermore, establishment of a Level A IVIVC gives confidence in the use of dissolution
212 testing as a change control tool.

213 Validation of a Level A IVIVC involves showing that it is sufficiently predictive. A Level A IVIVC is
214 established based for example on a deconvolution technique, in which *in vivo* absorption or *in vivo*
215 dissolution can be predicted from *in vitro* data and not C_{max} and AUC (detailed in Annex 2). A validated
216 Level A IVIVC allows the use of the associated *in vitro* dissolution test as a surrogate for an *in vivo* study,
217 as the resulting *in vivo* concentration-time profile can be predicted using the *in vitro* dissolution data and
218 the IVIVC equation. Implicit in this approach is that (1) such an IVIVC can only be reliably used for
219 interpolation (explained below) and (2) a single IVIVC model must be applicable to all formulations used
220 in its development and validation.

221 Note that an IVIVC cannot serve as a basis for claiming bioequivalence between products from different
222 MA applicants, based on *in vitro* data only.

223 An IVIVC model should be used for interpolation within the range of data used in its development, rather
224 than extrapolation outside of the range over which it is known to apply. This principle is particularly
225 important for regulatory applications, such as justification of dissolution specification and biowaivers.
226 This has important implications for the choice of formulations to be included in an IVIVC study.

227 It is generally recommended to use formulations with widely varying *in vitro* dissolution profiles for IVIVC
228 development and validation, since utilising formulations with only small differences in their *in vitro*
229 dissolution profiles will limit the scope for widening of the specification range and the range for which a
230 biowaiver can be justified. However, it is acknowledged that different release mechanisms or other
231 biopharmaceutical factors may come into play at the formulation extremes, impacting on the relationship
232 between *in vitro* and *in vivo* drug release and precluding generation of a single IVIVC equation which
233 describes the behavior of all formulations within the range proposed for a biowaiver. Therefore,
234 formulations should be chosen such that the same release mechanism is likely to control both the *in vitro*
235 and *in vivo* release of drug. This will tend to limit the range of *in vitro* dissolution profiles used in practice
236 for IVIVC development and validation.

237 If an extreme formulation (i.e. one with the fastest or slowest *in vitro* dissolution of the formulations used
238 in the IVIVC) is subsequently chosen for further development, it is advisable to extend the IVIVC
239 validation range by generating *in vivo* data for another formulation (yet faster or slower, as the case may

240 be) and using these data for external validation of the existing IVIVC or for redevelopment and validation
241 of a new IVIVC.

242 **2.2. Setting specifications**

243 The specification should be set using a discriminatory dissolution test.

244 In general, a minimum of three points should be included in the specification on *in vitro* dissolution of an
245 oral prolonged release product: an early time point to exclude dose dumping and/or to characterise a
246 loading/initial dose (typically 20 to 30% dissolved), at least one point to ensure compliance with the
247 shape of the dissolution profile (around 50% dissolved) and one to ensure that the majority of the active
248 substance has been released (generally more than 85% dissolved i.e. Q=80 %).

249 For drug products showing a zero order release a specification of the dissolution rate/time for a given time
250 interval may be more appropriate than the cumulative amount dissolved at a distinct time point. In cases
251 where a zero order release kinetic is combined with a variable lag time, such a specification is mandatory.

252 The acceptable variation allowed around each time-point (upper and lower limits), can be determined in
253 different ways:

254 a. No IVIVC:

255 The tolerance limits may be derived from the spread of *in vitro* dissolution data of batches with
256 demonstrated acceptable *in vivo* performance (biobatch(es)), or by demonstrating bioequivalence
257 between batches at the proposed upper and lower limit of the dissolution range (the so-called
258 "side-batch" concept).

259 Normally, the permitted range in release at any given time point should not exceed a total numerical
260 difference of $\pm 10\%$ of the labelled content of active substance (i.e. a total variability of 20%: a
261 requirement of $50 \pm 10\%$ thus means an acceptable range from 40-60%), unless a wider range is
262 supported by a bioequivalence study or a validated IVIVC.

263 b. Established Level A IVIVC:

264 The specification should be set using a discriminatory dissolution test. A validated Level A IVIVC allows
265 *in vitro* dissolution data (in this case, proposed rather than observed data) to be used as a surrogate to an
266 *in vivo* study of formulations at the proposed dissolution specification limits. Dissolution profiles are
267 generated from the proposed limits using an appropriate mathematical function (Weibull function, Hill, etc
268 as justified by the behaviour of formulations tested during product development) or, normally less
269 usefully, based on release at different time points. The entire plasma concentration-time profile is
270 calculated for the proposed upper and lower dissolution limits and the observed *in vitro* dissolution data
271 for the to-be-marketed (reference) formulation utilising the validated IVIVC. The corresponding C_{max}
272 and AUC values are calculated for the proposed lower and upper limits and the reference formulation and
273 the ratios calculated (upper to lower, upper to reference and lower to reference).

274 The guiding principle of specification setting is that all batches within the lower and upper dissolution
275 specification limits should be bioequivalent to one another. When bioequivalence is based on *in vivo*
276 data, the acceptance range for the maximum difference in comparative data is 80-125%, based on
277 confidence intervals around the mean C_{max} and AUC. Although some methods of IVIVC analysis quantify
278 biological variability (and allow prediction of confidence intervals), most methods predict mean
279 concentration-time data only. Therefore, for BE predicted based on mean data (by use of dissolution
280 data in lieu of *in vivo* data and supported by an IVIVC), the criteria for BE limits must necessarily be
281 tighter i.e., the difference between the C_{max} and AUC for the mean *in vivo* concentration-time data
282 predicted for the upper and lower dissolution specification must be less than 20%. Limits based on a

283 difference greater than 20% between the predicted C_{max} and AUC for the upper and lower dissolution
284 specifications must be justified.

285 For drugs that are absorbed throughout the gastrointestinal tract, the AUC is often similar for
286 formulations of widely varying dissolution rates and the specification is driven by C_{max} , rather than AUC.
287 In this case, the advantage of utilising an IVIVC for specification setting is that limits wider than +/- 10%
288 in cumulative dissolution at particular time points may be possible, as not every time point has the same
289 impact on C_{max} . The sensitivity of C_{max} to changes in dissolution depends on the pharmacokinetic
290 properties of the drug (the shorter the half-life the greater the sensitivity to changes in dissolution) and
291 the shape of the IVIVC relationship (i.e., whether *in vitro* or *in vivo* dissolution is faster).

292 **2.3. Control strategy**

293 General regulatory guidance on the establishment and justification of a control strategy for the drug
294 product is given in other relevant guidelines. Particular attention should however be paid to the control of
295 drug release from modified release drug products.

296 Pharmaceutical development should establish the link from pharmacokinetic parameters through *in vivo*
297 drug release to *in vitro* dissolution rate.

298 In an enhanced pharmaceutical development environment, compliance with the dissolution requirement
299 could be demonstrated by real time release testing (see

300 Guideline on Real Time Release Testing EMA/CHMP/QWP/811210/2009-Rev1). As the drug release rate
301 may be susceptible to scale-up effects, it is particularly important that the drug release rate prediction
302 algorithm is verified at the commercial scale.

303 **2.4. Variations to products**

304 The supporting data requirements for variations to the Marketing Authorisation will depend upon the
305 significance of the change, whether or not a Level A IVIVC exists and whether or not the dissolution
306 method/limits is to be changed. If bioavailability/bioequivalence data have not been submitted their
307 absence should always be justified.

308 When a Level A IVIVC has been established and the release specification is not changed, changes may be
309 accepted on the basis of *in vitro* data, the therapeutic index of the drug substance and predictive
310 capability of the IVIVC. In this case, waiver of a bioequivalence study should be based on comparison of
311 the predicted plasma concentration-time profiles and associated pharmacokinetic parameters (C_{max} ,
312 AUC and a shape parameter) for the formulations before and after changes, calculated utilising the *in vitro*
313 data and the validated IVIVC.

314 In general, bioavailability/bioequivalence data are needed for products with an established Level B or C
315 correlation or no IVIVC, unless justification is provided for absence of such data.

316 **3. Delayed release dosage forms**

317 Several delayed release dosage forms have been identified by the Ph.Eur.: gastro-resistant capsules,
318 tablets and granules. In this section, specific guidance is provided for gastro-resistant dosage forms.
319 Products based on other principles can also often be classified as delayed release dosage forms, including
320 those designed to release in a specific area of the gastrointestinal tract in response to a specific trigger
321 (e.g. enzymes) or at a specific time after ingestion. Although the principles described herein for the
322 pharmaceutical development, specifications and control strategy are also generally relevant for other

323 delayed release dosage forms, specific guidance for those dosage forms would have to be developed
324 based on the relevant formulation principle and mechanism of release.

325 Note that in addition to the points addressed below, many of the principles discussed under paragraph 2
326 are also relevant to delayed release dosage forms.

327 **3.1. Development pharmaceuticals**

328 A summary of the bioavailability studies should be given. The data should include information on
329 pharmacokinetics ($AUC_0 \rightarrow t_{last}$, $AUC_0 \rightarrow \infty$, C_{max} , and other relevant parameters; for generic products
330 also the point estimates and 90% confidence intervals), manufacturing sites and dates, batch sizes and
331 numbers, formulations and dissolution results of the batches used.

332 The rationale for the delayed release should be given, e.g. the protection of the gastric mucosa, the
333 protection of the active substance against the influence of acidic gastric medium or intended release of
334 the active substance in a predefined segment of the gastro-intestinal tract for local treatment, etc.

335 The mechanism of release and choice of the excipient(s) responsible for the delayed release should be
336 discussed e.g. targeting release at a given pH, susceptibility to enzymatic attack, erosion with time etc.

337 Pharmaceutical development should establish the link from pharmacokinetic parameters through *in vivo*
338 drug release to *in vitro* dissolution rate.

339 In principle two different types of formulations can be distinguished for delayed release products with
340 respect to the behaviour in the stomach:

- 341 • single unit non-disintegrating dosage forms;
- 342 • disintegrating dosage forms containing multiple units of pellets.

343 The development of single unit non-disintegrating gastroresistant dosage forms is generally discouraged
344 for gastroresistant products since their residence time in the stomach is unpredictable and in general
345 longer than disintegrating dosage forms which contain multiple units of pellets. Therefore, such single
346 unit non-disintegrating dosage forms are liable to a higher risk of dose-dumping and/or erratic
347 concentration profiles.

348 If the SmPC requires the co-administration with food or does not exclude the co-administration with food,
349 gastro-resistance should also be tested at a higher pH (e.g. in the range 3-5) for both single unit
350 non-disintegrating and disintegrating dosage forms with multiple units to determine resistance to release
351 in the fed stomach. Most meals will temporarily buffer the pH in the stomach to 3 or above, so pH 2 would
352 not be a sufficiently challenging test.

353 **3.2. Setting specifications**

354 At least two points should be included in the specification on *in vitro* dissolution of a gastroresistant
355 product: an early time point to exclude release in the acidic medium (less than 10% dissolved after 2
356 hours) and one to ensure that the majority of the active substance has been released in a (near) neutral
357 medium (see Ph. Eur.) It is emphasized that gastroresistance must be demonstrated for two hours or
358 more. With regard to acceptance criteria for continued testing, reference is made to the Ph. Eur..

359 **3.3. Control strategy**

360 Regulatory guidance on the establishment and justification of a control strategy for the drug product is
361 provided elsewhere. Particular attention should be paid to the control of critical quality attributes that are
362 responsible for the delayed drug release, e.g. the integrity of a gastro-resistant coating.

363 Pharmaceutical development should establish the link from pharmacokinetic parameters through *in vivo*
364 drug release to *in vitro* dissolution rate. In an enhanced pharmaceutical development environment,
365 compliance with the dissolution requirement could be demonstrated by real time release testing (see
366 Guideline on Real Time Release Testing EMA/CHMP/QWP/811210/2009-Rev1). As the principle for
367 controlling the drug release in a delayed release dosage form may be susceptible to scale-up effects, it is
368 particularly important that the design space is verified at the full commercial scale.

369 **3.3 Variations to products**

370 Since the *in vitro* test on gastro-resistance for delayed release dosage forms is considered relevant to the
371 *in vivo* situation, changes in the excipients responsible for delayed release in such products can be
372 supported by *in vitro* data only, where justified. Profiles of release after gastro-resistance testing should
373 of course be unchanged.

374 **ANNEX 1**

375 **Glossary**

376 Biobatch:

377 Batch used in a bioavailability/bioequivalence study or in clinical testing showing acceptable
378 performance; the size of this batch is at least pilot scale, i.e. for oral solid dosage forms at least 10 % of
379 full production scale or 100.000 units, whichever is larger

380 Conventional release dosage form:

381 Preparations showing a release of the active ingredient which is not deliberately modified by special
382 formulation and/or manufacturing method. In case of a solid dosage form, the dissolution profile of the
383 active ingredient depends essentially on the intrinsic properties of the active ingredient.

384 Equivalent term: Immediate release dosage form

385 Convolution:

386 Prediction of plasma drug concentrations using a mathematical model based on the convolution integral,
387 e.g. the following convolution integral may be used to predict plasma concentration (c(t)) resulting from
388 the absorption rate time course (rabs); The function c \bar{d} represents the concentration time course that
389 would result from the instantaneous absorption of a unit amount of drug and is typically estimated from
390 i.v. bolus data:

$$391 c(t) = \int_0^t c\bar{d}(t-u) rabs(u) du$$

392 Deconvolution:

393 Estimation of the time course of drug input (usually *in vivo* absorption or dissolution) using a
394 mathematical model based on the convolution integral; e.g. the absorption rate time course (rabs) that
395 resulted in the plasma concentration (c(t)) may be estimated by solving the following convolution integral
396 for rabs. The function c \bar{d} represents the concentration time course that would result from the
397 instantaneous absorption of a unit amount of drug and is typically estimated from i.v. bolus oral solution,
398 suspension or rapidly releasing immediate release dosage forms data:

$$399 c(t) = \int_0^t c\bar{d}(t-u) rabs(u) du$$

400 Delayed release dosage form:

401 Modified release dosage forms showing a release of the active ingredient which is delayed. Delayed
402 release is achieved by special formulation design and/or manufacturing method. The release of the active
403 substance is delayed for a predefined period after administration or application of the dosage form and
404 then releases as a conventional dosage form resulting in a lag time without any change in other
405 pharmacokinetic parameters.

406 External predictability:

407 Evaluation of predictability using a new data set then the ones on which the IVIVC is established (how well
408 predicts the model the data)

409 Internal predictability:

410 Evaluation of predictability using the initial test data set on which the IVIVC is established (how well
411 describes the model the data used for establishing the IVIVC).

412 Mean absorption time:

413 Time required for drug to reach systemic circulation from the time of drug administration = mean time
414 involved in the *in vivo* release and absorption processes as they occur in the input compartment:

415
$$\text{MAT} = \text{MRT}_{\text{oral}} - \text{MRT}_{\text{i.v.}}$$

416 Mean *in vitro* dissolution time:

417 The mean time for a drug to dissolve *in vitro*:

418
$$\text{MDT}_{\text{vitro}} = \int_0^{\infty} (M^{\infty} - M(t)) dt$$

419
$$M^{\infty}$$

420 Mean *in vivo* dissolution time:

421 The mean time for a drug to dissolve *in vivo*:

422
$$\text{MDT}_{\text{solid}} = \text{MRT}_{\text{solid}} - \text{MRT}_{\text{solution}}$$

423 Mean *in vivo* residence time:

424 The average time for a drug to reside in the body:

425
$$\text{MRT} = \text{AUMC} / \text{AUC}$$

426 Modified release dosage forms:

427 Preparations where the rate and/or place of release of the active ingredient(s) is different from that of the
428 conventional dosage form administered by the same route. This deliberate modification is achieved by
429 special formulation design and/or manufacturing method. Modified release dosage forms include
430 prolonged release, delayed release, pulsatile release and accelerated release dosage forms.

431 (It should be noted that pulsatile and accelerated release dosage forms are not covered by the current
432 guideline)

433 Percent prediction error:

434
$$\%PE = [(\text{observed value} - \text{predicted value}) / \text{observed value}] \times 100$$

435 Prolonged release dosage forms:

436 Modified release dosage forms showing a slower release than that of the conventional release dosage
437 form administered by the same route. Prolonged release is achieved by special formulation design/and/or
438 manufacturing method.

439 Equivalent term: extended release dosage form

440 Release controlling excipient:

441 Excipient with determining effect on the release of the active substance

442 Side batch:

443 Batches representing the intended upper and lower *in vitro* release specification derived from the defined
444 manufacturing process by setting process parameters within the range of maximum variability expected
445 from process validation studies

- 446 Sink conditions:
- 447 May be assumed if the amount of substance in solution at the end of the dissolution test does not exceed
448 30% of the saturation concentration
- 449 Statistical moments:
- 450 These are parameters that describe the characteristics of the time courses of plasma concentration (area,
451 mean residence time and variance of mean residence time) and of urinary excretion rate (Journal of
452 Pharmacokinetics & Biopharmaceutics, vol 6(6), 547, 1978)
- 453 Zero order release
- 454 The drug release rate is independent of time.

455 ANNEX 2

456 1. *In-vivo - in-vitro* correlations (IVIVC)

457 A number of techniques may be employed in order to establish an IVIVC. The following levels can be
458 defined:

459 Level A: representing a point-to-point relationship between the *in vitro* dissolution curve of the product
460 and the *in vivo* dissolution curves generated by deconvolution of plasma level data (Wagner-Nelson,
461 Loo-Riegelman, numeric deconvolution) or by other appropriate methods (e.g., modeling approaches
462 based on convolution or differential equations using average data or population pharmacokinetic
463 modeling).

464 Level B: representing a one point relationship between: a) the mean *in vitro* dissolution time of the
465 product and either the mean *in vivo* residence time or the mean *in vivo* dissolution time by using the
466 principles of statistical moment analysis; or b) the *in vitro* dissolution rate constant versus the absorption
467 rate constant derived.

468 Level C: representing a one point relationship between the amount dissolved *in vitro* at a particular time
469 and one mean pharmacokinetic parameter, e.g. AUC, C_{max} or T_{max} ; if one or several pharmacokinetic
470 parameters correlate to the amount of drug dissolved at several time points of the dissolution profile, a
471 multiple Level C correlation has been established.

472 2. Developing an IVIVC

473 2.1. Level A

474 Recommendations and considerations around the design of an IVIVC study and subsequent IVIVC data
475 analysis can be found in Section II of this Note for Guidance (Pharmacokinetic and Clinical Evaluation;
476 CPMP/EWP/280/96 Corr). Generally, two or more formulations with sufficiently different dissolution
477 profiles and an appropriate reference formulation (for the purpose of deconvolution) with fast drug
478 release (e.g., intravenous administration, oral solution or immediate release formulation) are
479 administered in a cross over study in healthy volunteers. Parent drug levels are quantified as a function
480 of time in blood or plasma. The IVIVC can be modeled directly using plasma concentrations (one step
481 approach) or after deconvolution of the modified release formulation concentration-time profiles relative
482 to the immediate release formulation (two step approach). In order for *in vitro* dissolution test to serve as
483 a surrogate marker for *in vivo* behaviour and to be used as a change control tool normally a level A IVIVC
484 is required.

485 Initial testing of the formulations in a variety of different dissolution tests/conditions at the time of
486 product release allows identification of the dissolution test that provides the most suitable discrimination.
487 The *in vitro* dissolution testing time points for the formulations used in the IVIVC study should be of
488 sufficient frequency to fully characterise the dissolution profile, including the plateau (e.g., three
489 consecutive points differing by less than 5%). Fewer time points may be chosen for QC testing, but the
490 converse is not true: QC time points are not appropriate for the *in vitro* component of the IVIVC data set
491 since (1) sparse data may not allow accurate interpolation between points and (2) sampling stopped prior
492 to reaching a plateau translates into incomplete drug release and compromises IVIVC validation.

493 **2.2. Level B and C**

494 Generally, level B and C correlations are not useful for supporting major variations in the composition or
495 manufacturing process of the product but in setting specifications, multiple level C correlations could be
496 supportive.

497 A multiple level C correlation is developed through if a linear correlation can be established based on a
498 minimum of on the one hand three time points, between the amount dissolved at three or more
499 timepoints or three MDT's and on the other hand the corresponding AUC and, C_{max} for a number of
500 formulations with different *in vitro* dissolution rate profiles, MRT or any other suitable pharmacokinetic
501 parameter (multiple level C), *in vitro* data can be used to predict *in vivo* performance. It should be noted
502 that if a multiple level C correlation is achievable, then also the development of a Level A correlation is
503 feasible. A Level A IVIVC allows prediction of the entire plasma concentration-time profile (giving
504 valuable insight into the shape of the profile and time of maximum concentration) in addition to summary
505 pharmacokinetic parameters, such as C_{max} and AUC, while only the summary pharmacokinetic
506 parameters are predicted from a multiple level C correlation. As such, a Level A is the preferred approach.
507 Additionally, it should be noted that if a multiple level C correlation is achievable, a Level A correlation is
508 likely to be feasible.

509 **3. Evaluating the predictability of an IVIVC**

510 In view of the use of an IVIVC as a surrogate marker for *in vivo* performance, it should be verified that the
511 predictability of the *in vivo* performance of a product based on its *in vitro* dissolution profile is valid for the
512 *in vitro* dissolution rates covered by the IVIVC. This evaluation should focus on the estimation of the
513 predictive performance or, conversely, prediction error.

514 In this evaluation, two basic concepts are important:

515 the less data available for development and evaluation of the IVIVC, the more additional data needed for
516 the complete evaluation of the predictability of the IVIVC

517 the formulations studied should differ adequately in release rate (e.g. $\geq 10\%$ dissolved) resulting in
518 substantial difference in the pharmacokinetic parameters of interest.

519 Methodology and reporting of predictability analysis are further discussed in Note for Guidance on
520 Modified Release Oral and Transdermal Dosage Forms: Section II (Pharmacokinetic And Clinical
521 Evaluation); CPMP/EWP/280/96 Corr).